



# Computational Modeling of Brainstem Stimulation

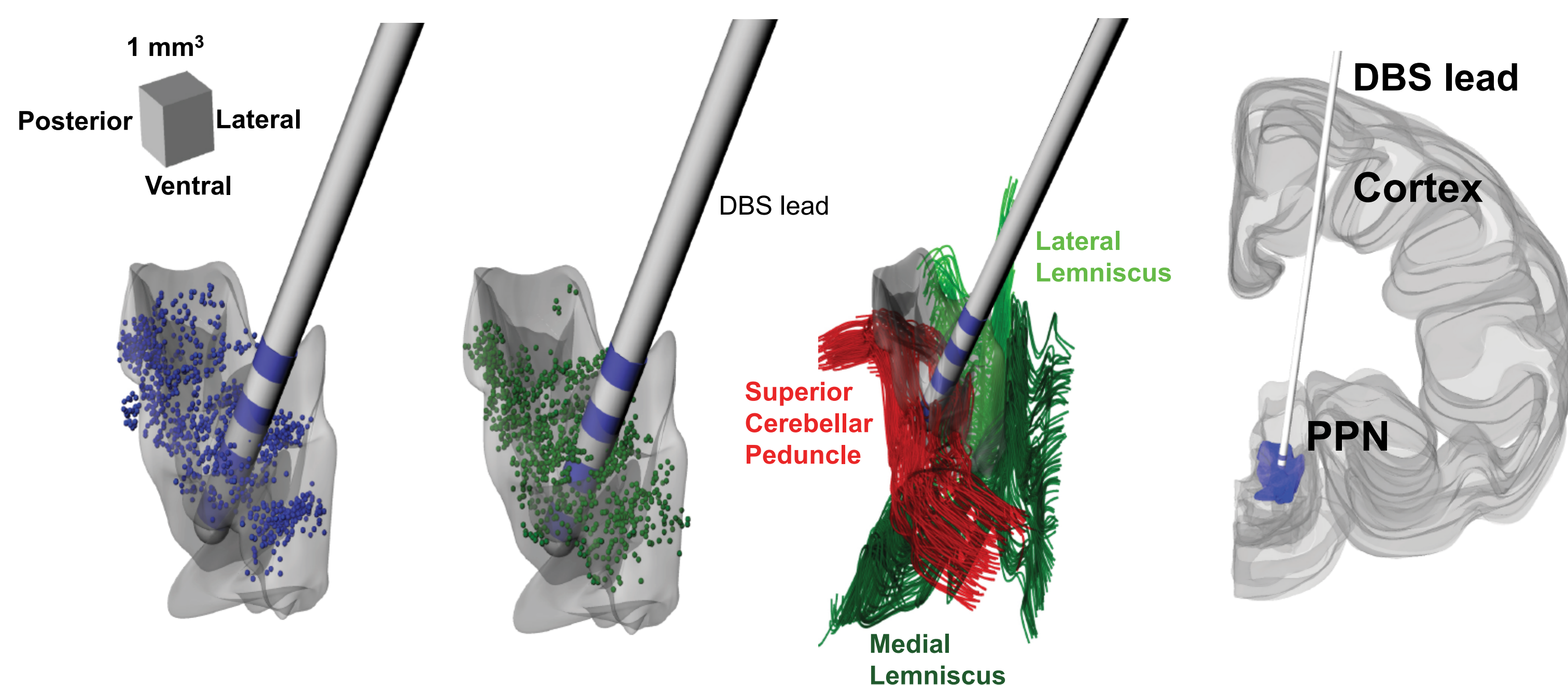
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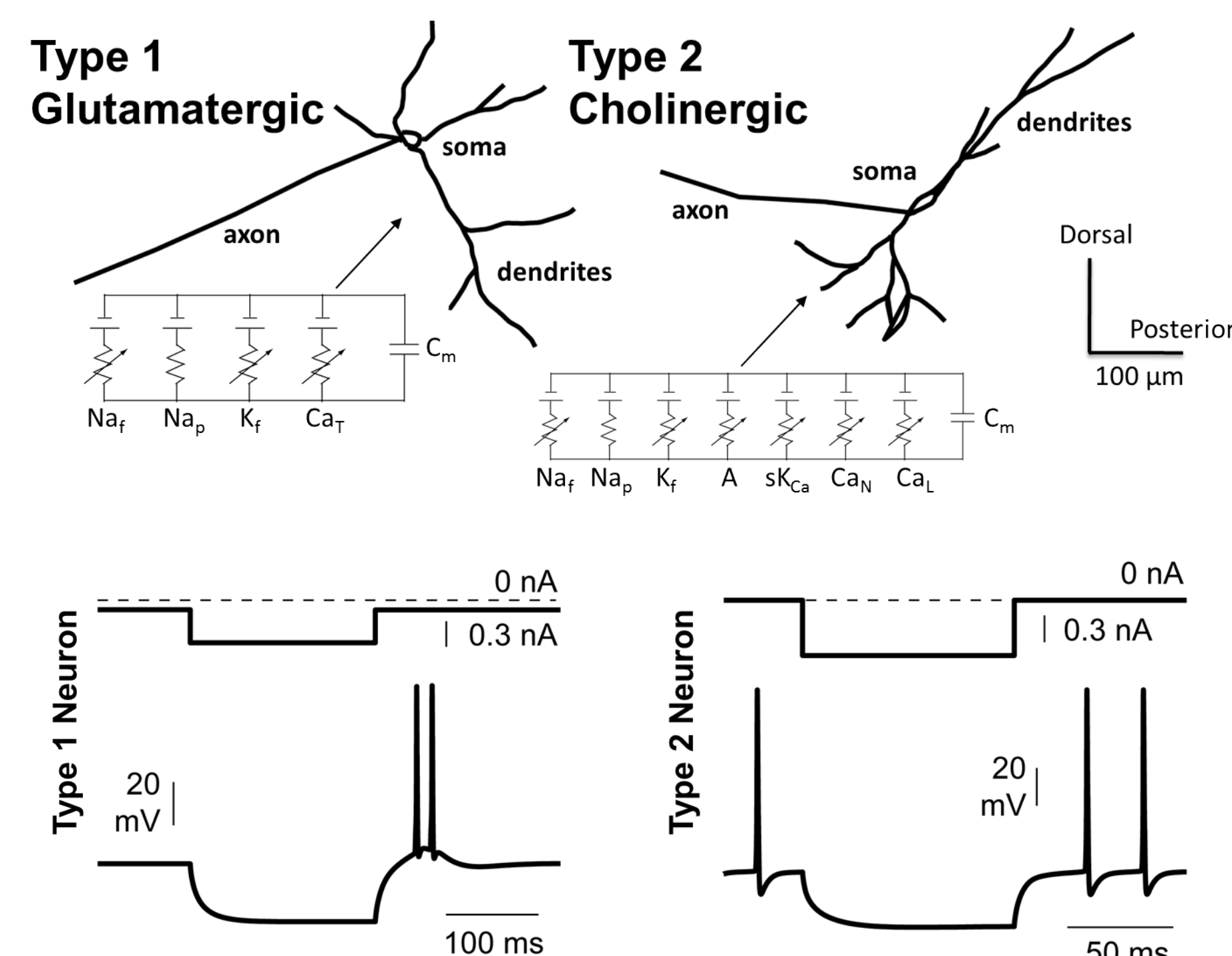
## Introduction

Modulation of the **Pedunculopontine nucleus (PPN)** using deep brain stimulation (DBS) is thought to improve gait disturbances in people with medication-refractory Parkinson's disease. However, previous studies have been inconclusive [1,2], with only some showing improvement in parkinsonian motor symptoms [3,4]. One of the primary challenges of PPN-DBS is avoiding activation of adjacent fiber pathways, which can evoke untoward side effects, including sensory discomfort. In this study we developed a **computational model of PPN-DBS** to predict the fiber pathways modulated by each stimulation setting. We developed a 3D model through reconstruction of the PPN, medial lemniscus (ML), lateral lemniscus (LL), and superior cerebellar peduncle (SCP) from non-human primate histological images. This anatomical framework was coupled with 1) a finite element model simulating the voltage field in the brain during DBS, and 2) a multi-compartment neuron model environment simulating the effects of DBS on PPN neurons and adjacent fiber pathways. These models provide a framework to predict how the implantation trajectory, lead position, and stimulation settings affect neural pathways in the brainstem.

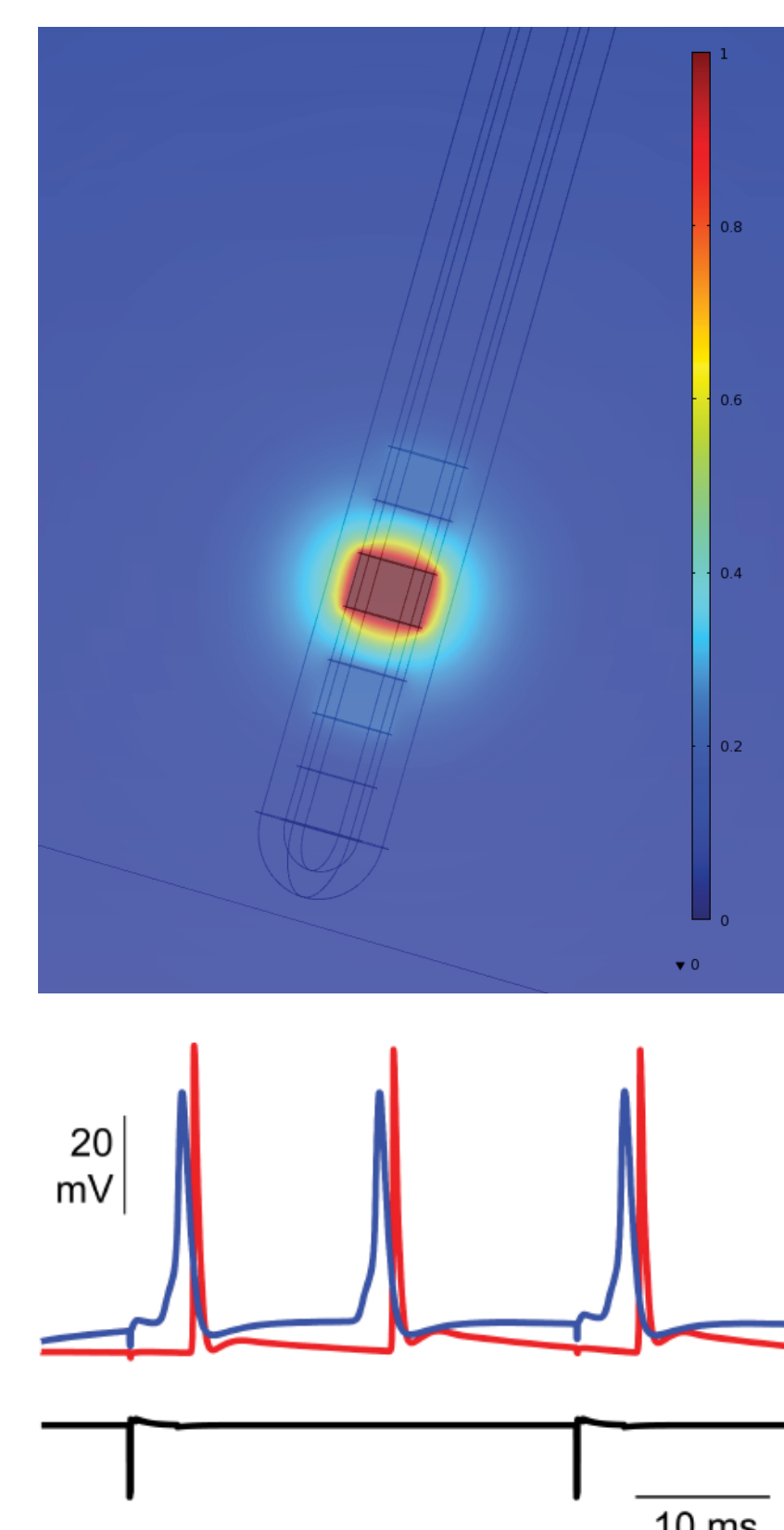
## Computational Methods



**Fig. 1.** The PPN is a challenging neurosurgical target for deep brain stimulation, given: 1) Its location deep within the brainstem (far right) 2) Its amorphous morphology (above) 3) Its variable distribution of cell types (above) 4) Its proximity to fibers of passage (above right)



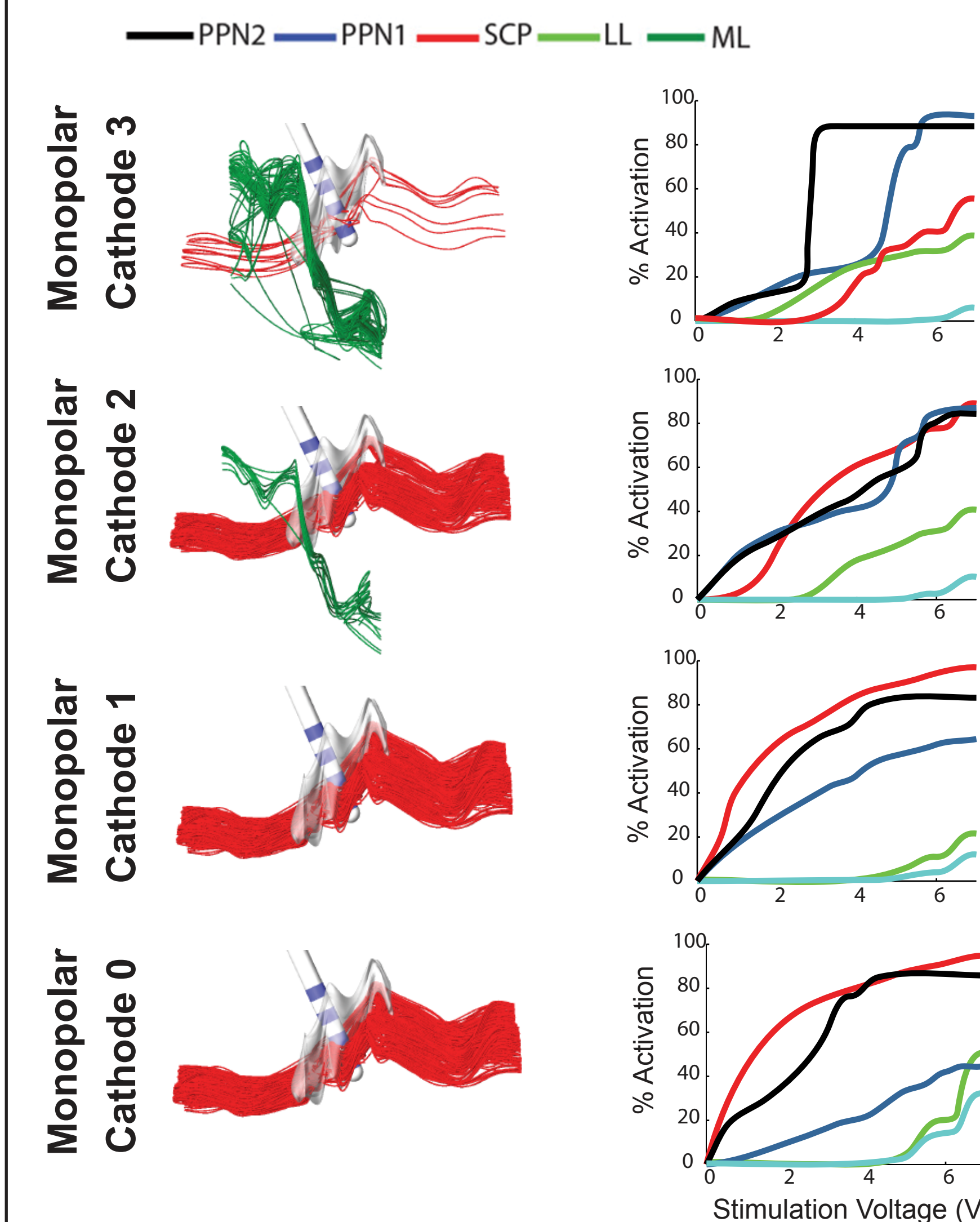
**Fig. 2.** PPN neuron models extended to the substantia nigra pars compacta, thalamus, and caudal brainstem [5,6]. Ion channel conductances were adapted in both PPN neuron models to reproduce the salient features of each cell type [7].



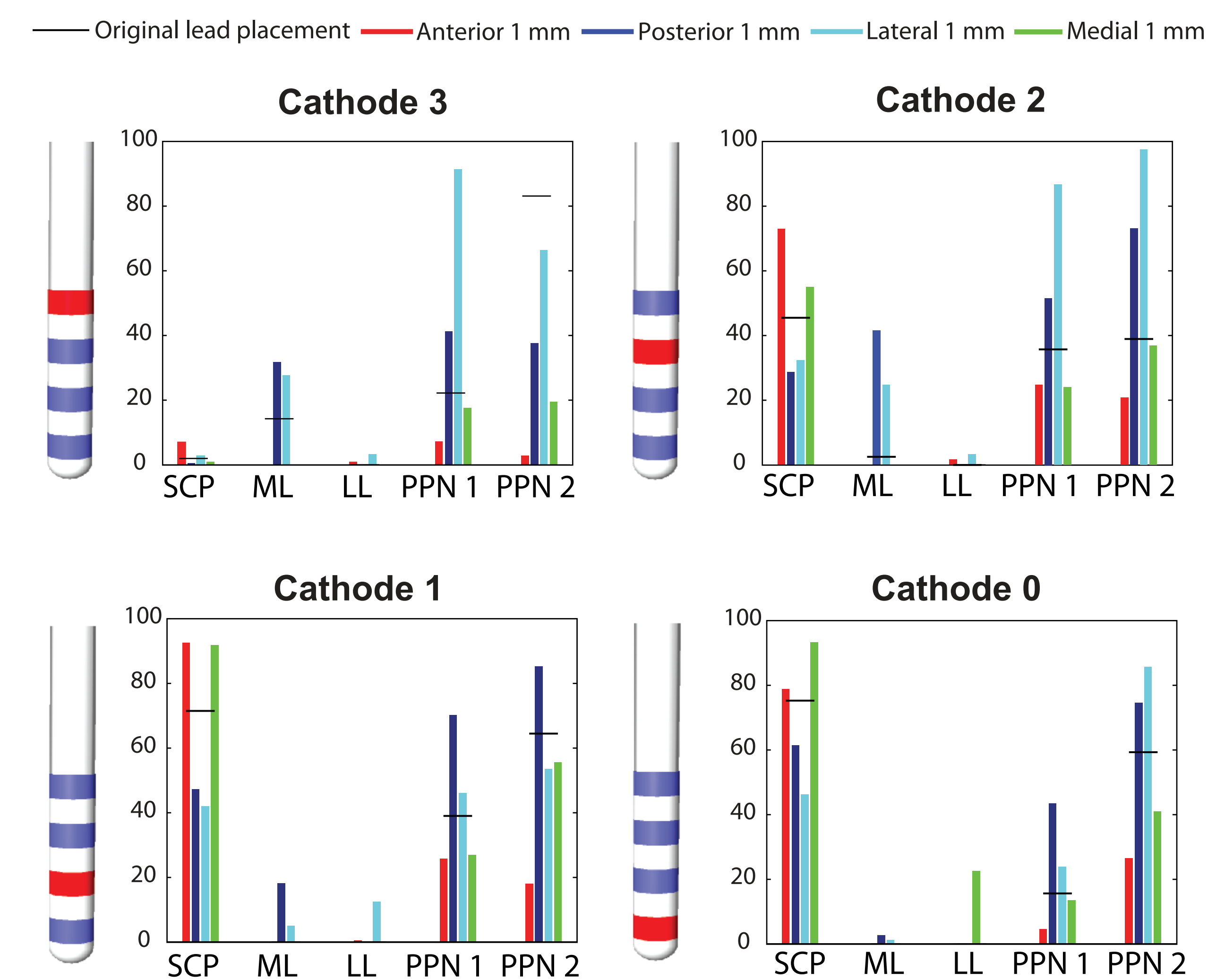
**Fig. 3.** Model dynamics were simulated for a range of electrode configurations and stimulation voltages using a 3D finite element model [8,9].

## Results

**Fig. 4.** Simulation results from a DBS lead implantation trajectory, showing activation plots (right) and fibers activated at 3 V (left).

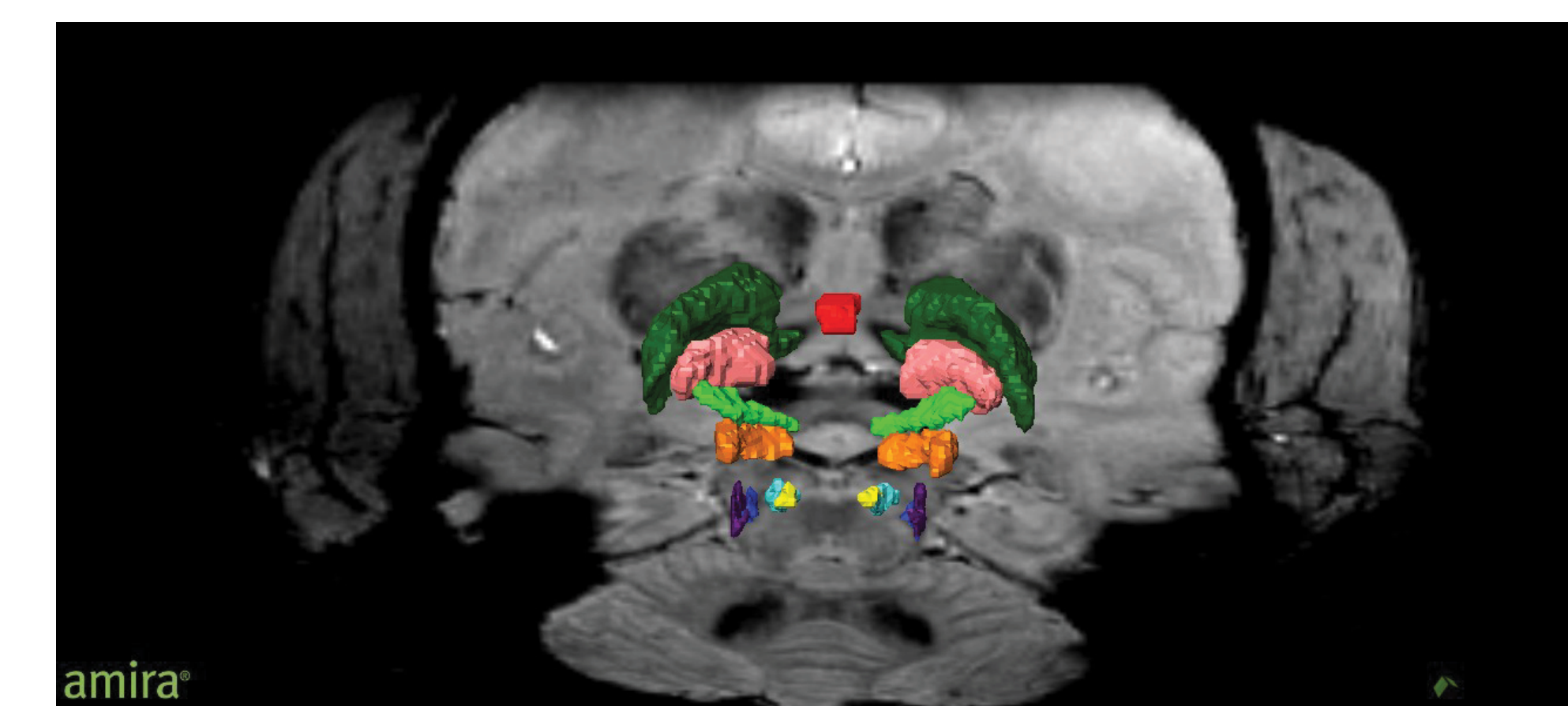
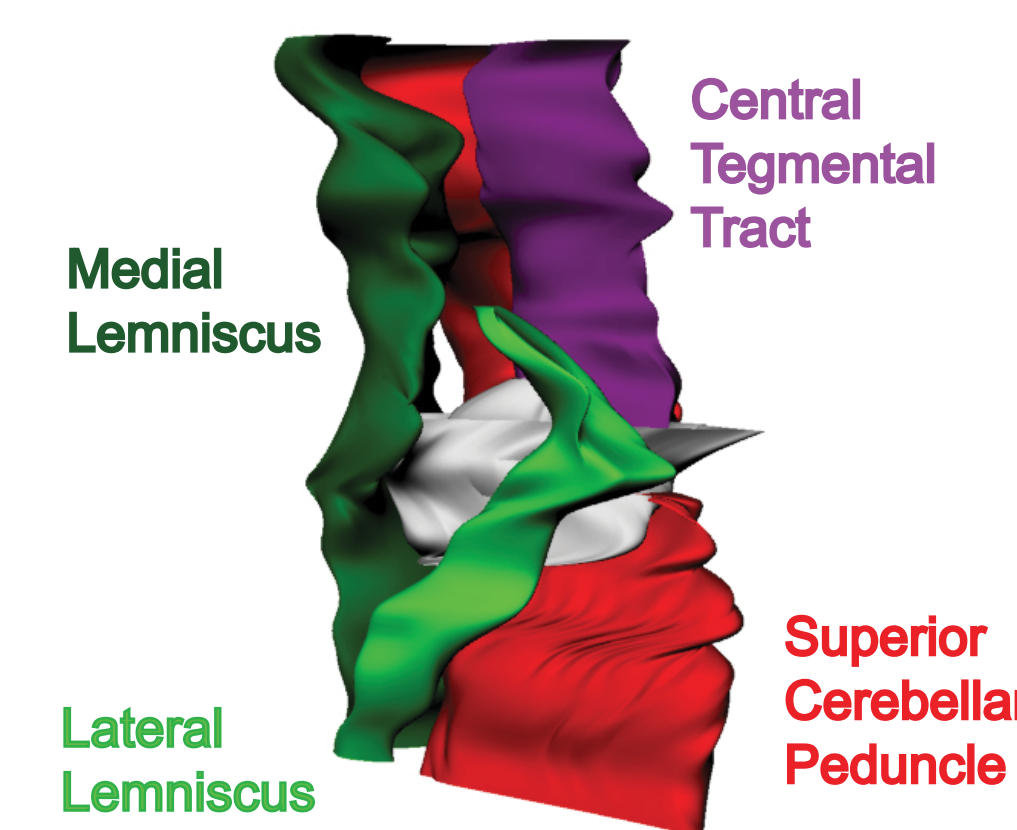


**Fig. 5.** Simulating implantation error. Results from moving lead implantation trajectory by 1 mm, displayed at 3 V activation voltage.



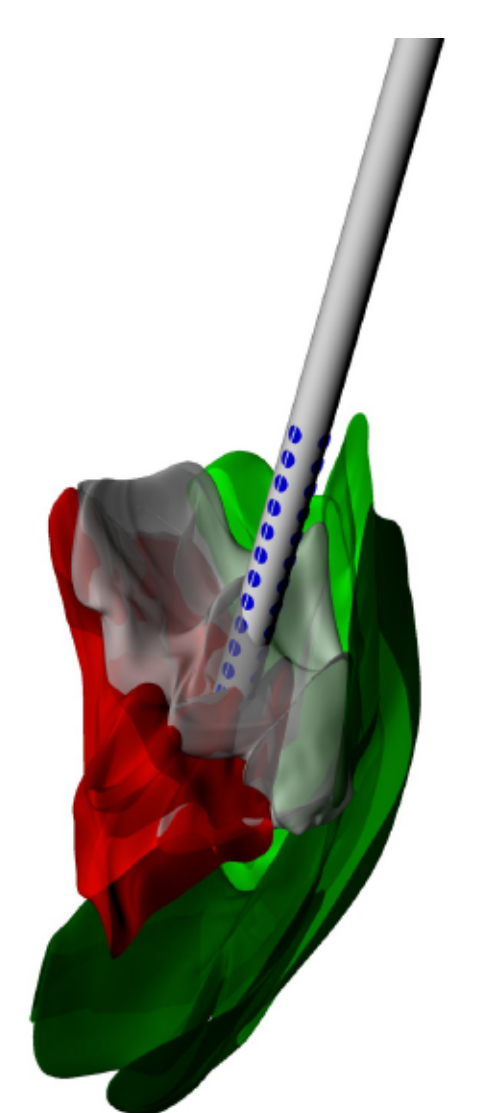
## Future Work

**Fig. 6.** The PPN, ML, LL, SCP, and the central tegmental tract pathways were reconstructed from human histological images. Future studies will compare **human PPN-DBS** to the model predictions shown above.



**Fig. 7.** Using 7T susceptibility-weighted imaging (SWI) of a non-human primate, we have segmented brainstem structures in order to model PPN-DBS using these reconstructions as a more accurate anatomical framework.

**Fig. 8.** A radially-segmented lead design can allow for current steering to more selectively activate PPN.



## Conclusions

Computational neuron models of PPN-DBS provide a theoretical framework by which to prospectively evaluate the effects of a range of DBS settings. Using an implant trajectory and lead design consistent with previous studies, we found:

- Both PPN cell types are affected by PPN-DBS, though to different degrees.
- Voltage thresholds for activating the SCP, ML and LL pathways ranged from (0.08-2.3 V), (1.6-4.2 V), and (4.0-5.6 V), respectively.
- Variations in the lead trajectory by 1 mm can have a large effect on activation profiles.
- Use of a radially-segmented lead design may allow for more selective stimulation of PPN.

## References

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